

# EVALUATION OF A SMALL FIELD OF VIEW SIPM ARRAY DETECTOR BASED ON A LGSO:Ce PIXELLATED SCINTILLATOR

**Stratos David, Eleftherios Fysikopoulos and Nektarios Kalyvas**

Department of Biomedical Engineering, Technological Educational Institute of Athens, 122 10  
Athens, Greece

**1<sup>st</sup>**

**EUROPEAN  
CONGRESS OF  
MEDICAL  
PHYSICS**

**September 1-4, 2016**  
Eugenides Foundation  
Athens-Greece

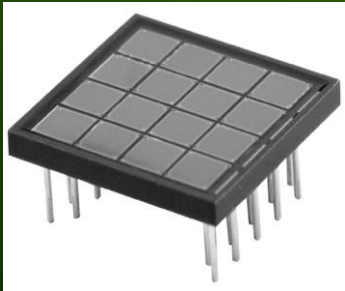
# Purpose

- ✔ The aim of this study is to investigate the behavior of the ArraySL-4 (4x4 array) silicon photomultiplier array coupled to a 6x6 LGSO:Ce pixellated scintillator, for possible applications in small field of view PET imaging detectors.
- ✔ Evaluation was carried out with  $^{137}\text{Cs}$  radioactive source and results regarding energy resolution and peak to valley ratio are presented.

# Introduction

- ✓ Silicon photomultipliers are used in dedicated small field of view animal imaging detectors (i.e in those used to head PET/MR studies in mice) due to their small size and flexibility.
- ✓ LGSO:Ce scintillator crystal is based on a mixture of LSO:Ce and GSO:Ce orthosilicates and has high density of  $7 \text{ g/cm}^3$ , high light output ( $\sim 32000 \text{ ph/MeV}$ ) and fast scintillation decay time ( $\sim 40 \text{ ns}$ ).

# Materials and Methods I



- ArraySL-4 (4x4 element array of  $3 \times 3 \text{ mm}^2$  silicon photomultipliers) purchased by SensL company, Ireland.

Fig 1. SensL's Sipm array



- LGSO:Ce 6x6 scintillator array, with  $1.9 \times 1.9 \times 5 \text{ mm}^3$  crystal size elements purchased by Amcrys company, Ukraine.

Fig 2. LGSO:Ce scintillator array

## Materials and Methods II

- ✔ We have developed a symmetric resistive charge division circuit to read out the signal outputs of 4x4 pixel SiPM array reducing the 16 pixel outputs to 4 position signals.
- ✔ The 4 position signals were acquired using a free running sampling technique.
- ✔ An FPGA (Spartan 6 LX150T) was used for triggering and signal processing of the pulses acquired using free running Analog to Digital Converters.

# Results

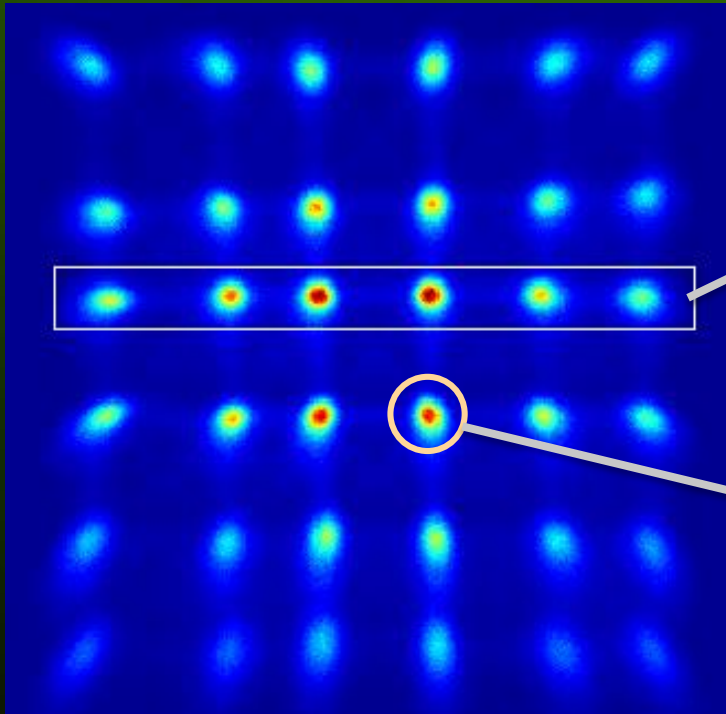


Fig 3. Raw image produced under 662 keV excitation at room temperature.

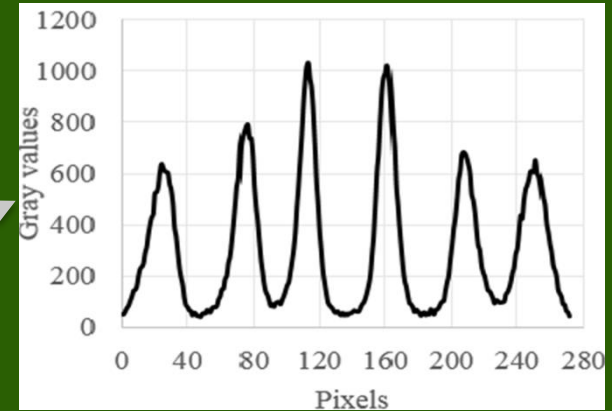


Fig 4. Horizontal profile of the pixel elements

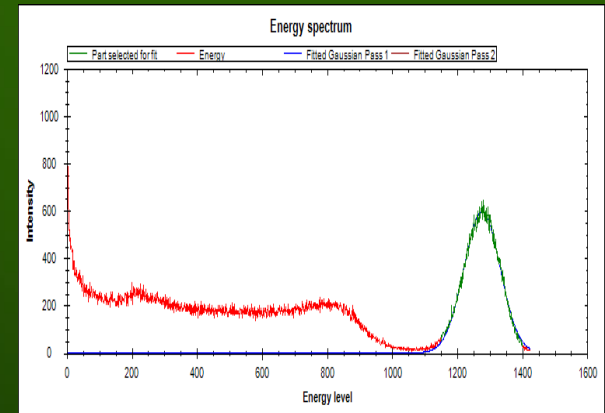


Fig 5. Energy spectrum of the central scintillator element.

## Conclusions

- ✔ Evaluation shows a clear visualization of all (64) discrete scintillator elements.
- ✔ The mean peak to valley ratio of the profiles on the image was measured equal to 13.
- ✔ The mean energy resolution was measured equal to 18%.

## References

1. Sidletskiy, O., Bondar, V., Grynyov, B., Kurtsev, D., Baumer, V., Shtitelman, Z., Tkachenko, S., Zelenskaya, O., Starzhinsky, N., Belikov, K., Tarasov, V., 2009. Growth of LGSO: Ce crystals by the czochralski method. *Crystallogr. Rep.* 54 (7), pp.1256-1260.
2. Buzhan, P., L. Filatov, A. Ilyin, V. Kantzerov, V. Kaplin, A. Karakash, F. Kayumov, S. Klemin, E. Popova, and S. Smirnov, (20B. Dolgoshein, 03) "Silicon photomultiplier and its possible applications." *Nucl. Instrum. Methods Phys. Res. A*, Vol. 504, pp.48-52.
3. Fysikopoulos E, Loudos G, Georgiou M, David S, Matsopoulos GA. Spartan 6 FPGA-based data acquisition system for dedicated imagers in nuclear medicine. *Meas Sci Technol* 2012; 23(12). <http://dx.doi.org/10.1088/0957-0233/23/12/125403>.
4. M. Streun ,G. Brandenburg , H. Larue, E. Zimmermann, K. Ziemons and H. Halling, (2001) "Pulse Recording by Free-Running Sampling", *IEEE Trans. Nucl. Sci.*, vol. 48, pp. 524-526,
5. V. Popov, S. Majewski and B. Welch, (2006) "A novel readout concept for multianode photomultiplier tubes with pad matrix anode layout", *Nucl. Instrum. Meth. A* , Vol. 567, p. 319
6. Yamamoto, S., Imaizumi, M., Watabe, T., Watabe, H., Kanai, Y., Shimosegawa, E., Hatazawa, J., 2010. Development of a Si-PM-based high-resolution PET system for small animals. *Phys. Med. Biol.* 55, pp. 5817-5831